

PHARMACOLOGICAL CHALLENGES AND ADVANCES IN CONTROLLED RELEASE DELIVERY OF PEPTIDE THERAPEUTICS

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Article Received: 17 March 2026 | Article Revised: 8 April 2026 | Article Accepted: 28 April 2026

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DOI: <https://doi.org/10.5281/zenodo.19997565>

How to cite this Article: Sneha S. Pawar, Isha C. Bachhav, Nandini A. Panda, Lina B. Bhoi, Bhavana B. Ahire, Nikhil M. Patil, Ghanshyam M. Chavan (2026) PHARMACOLOGICAL CHALLENGES AND ADVANCES IN CONTROLLED RELEASE DELIVERY OF PEPTIDE THERAPEUTICS. World Journal of Pharmaceutical Science and Research, 5(5), 539-565.



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ABSTRACT

Background: Peptide therapeutics have emerged as a significant class of modern pharmacological agents owing to their high target specificity, potent biological activity, and favorable safety profiles. However, their clinical application is substantially limited by inherent pharmacokinetic and pharmacodynamic challenges, including poor oral bioavailability, rapid enzymatic degradation, short plasma half-life, limited membrane permeability, and dependence on parenteral administration. **Objective:** This review aims to critically analyze the pharmacological challenges associated with peptide therapeutics and to highlight the role of controlled-release drug delivery systems in overcoming these limitations to improve therapeutic efficacy and patient compliance. **Methods:** A comprehensive literature-based analysis was conducted focusing on the physicochemical, pharmacokinetic, and pharmacodynamic barriers of peptide drugs. Various controlled-release delivery platforms, including polymeric microspheres, nanoparticles, hydrogels, lipid-based carriers, and depot systems, were systematically evaluated along with recent advances such as chemical modification strategies, stimuli-responsive systems, and nanotechnology-based approaches. **Results:** Controlled-release delivery systems significantly enhance peptide stability, prolong systemic circulation, and enable sustained and site-specific drug release, thereby improving bioavailability and reducing dosing frequency. Advanced delivery technologies demonstrate promising outcomes in overcoming enzymatic degradation, rapid clearance, and distribution limitations. However, challenges such as maintaining peptide bioactivity, controlling release kinetics, preventing burst release, immunogenicity concerns, and large-scale manufacturing complexities remain critical barriers to clinical translation. **Conclusion:** Controlled-release systems represent a pivotal strategy in optimizing peptide drug delivery and bridging the gap between preclinical potential and clinical application. Future advancements integrating nanotechnology, artificial intelligence, and personalized medicine approaches are expected to further enhance the therapeutic performance of peptide-based drugs and expand their clinical utility.

KEYWORDS: Peptide therapeutics, Controlled-release drug delivery, Pharmacokinetics, Nanocarriers, Hydrogels, Depot systems, Drug stability, Targeted delivery.

1. INTRODUCTION

Peptide drugs have emerged as a critically important class of therapeutic agents in modern medicine due to their unique biochemical properties, which enable high target specificity, potent biological activity, and favorable safety profiles compared with many traditional small molecules and biologic therapies. Therapeutic peptides are typically composed of short chains of amino acids (≈ 500 – $5,000$ Da), offering advantages such as precise interaction with physiological targets and reduced off-target effects. These attributes make them especially valuable for modulating complex biological processes that are challenging to address with conventional small molecules.^[1,2] The growing number of licensed peptide medications reflects the clinical significance of peptide therapies. More than 80 peptide medications have been approved globally as of 2023, covering a wide range of therapeutic categories such as neurological, cardiovascular, infectious, and metabolic problems. Additionally, more than 170 peptide candidates are currently undergoing clinical development, and many more are in preclinical phases, demonstrating a strong pipeline and rising translational interest.^[1]

Examples such as glucagon-like peptide-1 receptor agonists (e.g., liraglutide and semaglutide) have revolutionized the treatment of type 2 diabetes and obesity through improved glycemic control and cardiovascular advantages. Peptide medications have had a substantial impact on the treatment of complicated disorders. These medication classes represent a significant portion of the peptide therapeutics market in addition to demonstrating the clinical value of peptide modalities.^[1,3] Together, peptide medications brought in over USD 70 billion in sales worldwide in 2019—nearly twice as much as in the early 2010s—reflecting both commercial expansion and clinical uptake.^[1] Peptide medications have historically had pharmacokinetic difficulties, such as low oral bioavailability, quick enzymatic breakdown, a brief plasma half-life, and restricted membrane permeability, despite their potential.^[4] However, recent developments in peptide chemistry and delivery methods—such as cyclization, lipidation, PEGylation, the use of artificial amino acids, and sustained-release formulations—have significantly enhanced pharmacological performance and stability, opening up new clinical applications.^[2] Peptide drug discovery and development are currently being accelerated by integrative methodologies that combine computational modeling, rational design, high-throughput screening, and creative delivery platforms. By addressing unmet medical requirements across many disease landscapes, such collaborative innovation supports peptides' role as a cornerstone of next-generation pharmacotherapy and continues to broaden their therapeutic spectrum.^[1]

2.1. Limitations of Conventional Peptide Administration

Because of their strong biological activity, high specificity, and advantageous safety profiles, peptide-based medicines have drawn a lot of interest in contemporary pharmacotherapy. Despite these benefits, a number of intrinsic restrictions related to peptide medicines' traditional means of delivery continue to severely impede their clinical translation and broad use. Their physicochemical characteristics, biological instability, pharmacokinetic behavior, and patient-related factors are the main causes of these difficulties.

2.1.1. Poor Oral Bioavailability

The incredibly low oral bioavailability of traditional peptide administration is one of its most significant drawbacks. Proteolytic enzymes found throughout the gastrointestinal tract, such as pepsin, trypsin, and chymotrypsin, may easily break down peptides. Furthermore, denaturation of peptide structures and chemical instability might be caused by the acidic stomach environment. Due to their high molecular size, hydrophilicity, and restricted capacity to pass through

the intestinal epithelium, even peptides that withstand enzymatic breakdown encounter substantial obstacles to absorption. As a result, oral administration produces relatively little systemic exposure, making it inappropriate for the majority of therapeutic peptides and requiring the use of alternate delivery methods.^[5-7]

2.1.2. Rapid Enzymatic Degradation and Short Biological Half-Life

Peptidases and proteases in circulation quickly break down peptide medications after systemic delivery, resulting in brief plasma half-lives that frequently range from minutes to a few hours. Furthermore, because of their great aqueous solubility and low molecular weight, peptides are quickly cleared by the kidneys. The length of therapeutic effectiveness is limited by this quick clearance, and regular doses is necessary to maintain optimal plasma concentrations. Such pharmacokinetic instability raises the possibility of dose-related side effects and therapeutic outcome variability in addition to decreasing treatment efficacy.^[8-10]

2.1.3. Dependence on Parenteral Administration

Conventional peptide therapies are mostly provided by parenteral routes, such as intravenous, subcutaneous, or intramuscular injection, due to low stability and absorption via non-invasive ways. Although these methods avoid gastrointestinal degradation and first-pass metabolism, they have a number of disadvantages, such as injection site pain, infection risk, and less patient compliance, especially in chronic illnesses requiring long-term therapy. Treatment is made more difficult and expensive by the requirement for sterile formulations, skilled medical staff, or frequent self-injection.^[11,12]

2.1.4. Limited Membrane Permeability

Because of their polarity, relatively large molecular size, and vulnerability to efflux transporters, peptides naturally have limited permeability across biological membranes. These traits prevent them from passively diffusing through endothelium and epithelial barriers, such as the blood–brain barrier, skin, and nasal mucosa. As a result, achieving therapeutically relevant concentrations at target sites remains challenging with conventional administration approaches, particularly for central nervous system or intracellular targets.^[13,14]

2.1.5. Immunogenicity and Off-Target Effects

Exogenous peptides that are administered repeatedly may cause immunological reactions, particularly if the peptide sequences are structurally altered during formulation or differ from their endogenous counterparts. Anti-drug antibody production can cause hypersensitivity responses, change pharmacokinetics, or decrease therapeutic efficacy. Peptides' structural flexibility may also lead to decreased receptor selectivity, which raises the possibility of off-target interactions and unexpected pharmacological consequences.^[15,16]

2.1.6. Manufacturing Complexity and High Cost-

In order to guarantee biological activity and batch-to-batch consistency, peptide medication development entails intricate synthesis, purification, and stabilization procedures that call for strict quality control. Production costs are greatly increased when comprehensive analytical characterisation is combined with advanced solid-phase peptide synthesis. These financial limitations restrict accessibility and present difficulties for large-scale manufacturing, especially in healthcare settings with low and intermediate incomes.^[17]

2.1.7. Limited Targeted Bio-distribution

Peptide medications are frequently distributed non-specifically throughout the body via conventional systemic administration, which results in less-than-ideal accumulation at the intended target site. This lack of site-specific distribution raises the risk of side effects by increasing systemic exposure and decreasing therapeutic efficacy. These restrictions highlight the requirement for sophisticated delivery methods that can improve regulated release patterns and targeted bio-distribution.^[18]

2.2. Rationale for Controlled Release Systems for Peptide Drugs

Because of their strong biological activity, excellent target specificity, and very low systemic toxicity, peptide therapies have become a significant class of pharmacologically active medicines. They are essential in the treatment of autoimmune illnesses, cancer, infectious diseases, metabolic problems, and hormone shortages. Nevertheless, adverse pharmacokinetic and pharmacodynamic characteristics when given in traditional dose forms severely limit the clinical utility of peptide medicines, notwithstanding their therapeutic potential. The development of controlled release drug delivery systems (CRDDS) specifically designed for peptide-based therapies is based on these problems.

2.2.1. Overcoming Short Biological Half-Life and Rapid Clearance-

The short plasma half-life of peptide medications is a significant pharmacological drawback, mainly because of their quick renal clearance and enzymatic breakdown by endo- and exopeptidases. Frequent dosing is required to maintain therapeutic levels since conventional immediate-release formulations cause strong peaks and quick decreases in plasma drug concentration. In order to maintain long-term, therapeutically effective plasma concentrations, controlled release devices are made to adjust the kinetics of drug release. This method improves overall treatment outcomes, reduces peak–trough swings, and increases pharmacodynamic stability.^[8,9,19]

2.2.2. Enhancement of Therapeutic Efficacy and Pharmacodynamic Stability

Peptide medications frequently have limited therapeutic windows, and even little variations in drug concentration can result in side effects or subtherapeutic effects. Peptides can be delivered at a predefined rate using controlled release methods, which guarantee consistent pharmacological efficacy and extended receptor engagement. Controlled release formulations improve receptor occupancy and signal regulation by preserving steady-state drug levels. This is especially important for hormones, growth factors, and neuropeptides that need constant physiological mimicking for maximum efficacy.^[5,7]

2.2.3. Reduction in Dosing Frequency and Improved Patient Compliance

Patient adherence is severely hampered by the frequent parenteral delivery, particularly when managing chronic illnesses. Injectable microspheres, biodegradable polymeric matrix, and depot injections are examples of controlled release delivery systems that lower the frequency of dosing from daily to weekly or even monthly intervals. In addition to improving patient compliance, this lessens the burden of healthcare, injection-site reactions, and discomfort associated with administration. Better long-term clinical results and slower disease progression are directly correlated with increased adherence.^[11,12,20]

2.2.4. Protection from Enzymatic and Chemical Degradation

Because of enzymatic attack and chemical degradation routes such oxidation, deamidation, and aggregation, peptides are intrinsically unstable in physiological conditions. Peptide molecules can be protected from severe biological

conditions and early breakdown by being encapsulated in protective carriers using controlled release mechanisms. By extending peptide stability at the administration site and throughout systemic circulation, these methods preserve biological activity and lower the necessary dosage.^[14,17,18]

2.2.5. Optimization of Bioavailability and Site-Specific Delivery

Conventional systemic injection frequently results in limited accumulation of peptide medicines at the intended target location and non-specific dispersion. By enhancing drug concentration at the therapeutic target and reducing systemic exposure, controlled release platforms can be designed to distribute drugs in a localized, site-specific, or stimuli-responsive manner. In oncology, inflammatory diseases, and disorders of the central nervous system, where localized and prolonged peptide administration can greatly improve therapeutic index, this is especially helpful.^[15, 21]

2.2.6. Reduction of Systemic Toxicity and Adverse Effects

Immediate-release formulations with high peak plasma concentrations may raise the risk of immunogenic reactions and systemic adverse effects. By keeping drug levels within the therapeutic window for extended periods of time, controlled release devices reduce these hazards. Controlled administration improves safety and tolerability, which is essential for long-term peptide therapy, by lowering systemic fluctuations and preventing supratherapeutic peaks.^[10]

2.2.7. Facilitating Translation of Novel Peptide Therapeutics

Instead of lacking pharmacological activity, many attractive peptide candidates fail throughout clinical development because of poor pharmacokinetic performance. By enhancing in vivo stability, bioavailability, and patient acceptance, controlled release technologies offer a tactical platform to get over these translational obstacles. Therefore, controlled release techniques are essential for bridging the gap between peptide therapeutic preclinical success and clinical applicability.^[22]

3. Pharmacological Characteristics of Peptide Drugs to the Need for Controlled-Release Drug Delivery Systems

Peptide treatments provide special pharmacological benefits, such as strong biological activity and excellent target selectivity. However, when given using traditional dosage forms, their intrinsic physicochemical and biological limitations severely limit their therapeutic utility. By adjusting release kinetics, improving stability, and maximizing pharmacokinetic and pharmacodynamic profiles, controlled-release drug delivery devices have become a logical and essential way to get over these obstacles.

3.1. Molecular Size and Structural Instability: Need for Protective Controlled-Release Matrices

Peptide medications are structurally unstable under physiological and formulation settings due to their relatively large molecular size and conformational complexity. Peptides can undergo oxidation, deamidation, aggregation, and conformational unfolding, among other chemical degradation processes that can impair biological activity and boost immunogenic potential. Peptide molecules are protected from external stressors by controlled-release technologies, including polymeric carriers and encapsulation matrices. Controlled-release formulations improve structural integrity and maintain pharmacological action over extended periods of time by physically separating peptides from harsh physiological circumstances and limiting exposure to destabilizing elements.^[17,23]

3.2. Enzymatic Degradation and Short Half-Life: Need for Sustained and Prolonged Drug Release

Peptide drugs are structurally unstable in physiological and formulation conditions because their molecules are relatively big and their shapes are hard to understand. Peptides can break down chemically through processes like oxidation, deamidation, aggregation, and conformational unfolding. This can make them less effective in biological systems and more likely to cause an immune response. Controlled-release systems, particularly polymeric carriers and encapsulation matrices, provide a protective microenvironment that shields peptide molecules from external stressors. By physically isolating peptides from harsh physiological conditions and limiting exposure to destabilizing factors, controlled-release formulations enhance structural integrity and preserve pharmacological activity over prolonged durations.^[9,10,13]

3.3. Poor Membrane Permeability: Need for Prolonged Systemic Exposure

Peptide medications are mostly limited to parenteral administration due to their poor membrane permeability, which severely restricts their absorption and distribution across biological barriers. Instead of depending on quick absorption, controlled-release systems extend systemic exposure to make up for this restriction. Despite restricted membrane transport, depot formulations, injectable microspheres, and implantable systems guarantee sufficient bioavailability by continuously releasing peptides into the systemic circulation. Controlled-release systems enhance overall drug exposure and therapeutic efficacy by sustaining prolonged plasma levels without necessitating frequent or invasive administration.^[7,14]

3.4. Immunogenicity Concerns: Need for Reduced Peak Concentrations and Controlled Exposure-

Aggregation, repeated bolus dosing, and high peak plasma concentrations are frequently linked to immunogenic reactions to peptide medications. Supratherapeutic peaks that boost antibody formation and immune system recognition can be produced by traditional immediate-release formulations. By delivering peptides at regulated, sub-toxic concentrations for prolonged periods of time, controlled-release systems reduce the risk of immunogenicity. During long-term treatment, this steady and gradual exposure improves tolerability, minimizes aggregation at the injection site, and lowers immune stimulation. Consequently, controlled-release formulations improve therapeutic sustainability and safety.^[15,16]

4. Pharmacokinetic and Pharmacodynamic Challenges of Peptide Drugs to the Advantages of Controlled-Release Drug Delivery Systems

Although peptide therapeutics have strong pharmacological activity and high biological specificity, complicated pharmacokinetic and pharmacodynamic issues frequently impede their clinical translation. By modifying drug release profiles, enhancing stability, and maximizing systemic exposure, controlled-release drug delivery systems have become a logical solution to these constraints. The following section discusses the direct correlation between each PK/PD challenge and the associated benefit of controlled-release systems.

4.1. Absorption Barriers (Oral, Transdermal, Nasal Routes): Need for Prolonged and Protected Drug Availability

Because of their rapid clearance at the site of administration, poor membrane permeability, and enzymatic degradation, peptide drugs present significant absorption barriers when administered non-parenterally. The stratum corneum and mucociliary clearance, respectively, limit transdermal and nasal routes, whereas gastrointestinal proteases and epithelial tight junctions limit oral delivery. Bioavailability is low and very variable as a result of these barriers. By preserving

extended and localized drug availability at the administration site or within the systemic circulation, controlled-release systems make up for inadequate absorption. Encapsulation in injectable microspheres, depot formulations, or polymeric matrices guarantees prolonged peptide release, decreasing the need for quick absorption. Despite intrinsic absorption limitations, controlled-release systems improve overall bioavailability by prolonging the duration of drug exposure.^[5,7,24]

4.2. Distribution and Tissue Targeting Issues: Need for Sustained Exposure and Controlled Biodistribution-

Peptide medications frequently exhibit unfavorable distribution profiles after systemic administration because of their quick clearance, non-specific tissue uptake, and restricted penetration into target tissues. Because they are hydrophilic, they limit transmembrane transport and prevent accumulation at disease-specific locations, which leads to less-than-ideal receptor engagement and decreased pharmacodynamic efficacy. By sustaining constant plasma concentrations over extended periods of time, controlled-release drug delivery systems enhance tissue exposure and raise the likelihood of drug–target interactions. Furthermore, sophisticated controlled-release platforms can be designed for site-specific or localized delivery, improving therapeutic concentration at the target site and minimizing non-specific distribution. Thus, sustained release enhances the degree and duration of pharmacological action.^[13,14,25]

4.3. Rapid Clearance and Metabolic Instability: Need for Half-Life Extension and Reduced Elimination

The pharmacokinetic limitations of peptide drugs are characterized by rapid enzymatic degradation and renal clearance, which result in short plasma half-lives and fleeting therapeutic effects. Frequent dosing is required because immediate-release formulations frequently result in short exposure windows that are insufficient for sustained receptor activation. By offering continuous and regulated peptide release, controlled-release systems are especially made to combat rapid clearance and thereby increase the drug's apparent half-life. By preserving low, sustained systemic concentrations, encapsulation lowers renal elimination and shields peptides from rapid enzymatic degradation. This method lowers the frequency of doses, prolongs therapeutic action, and stabilizes pharmacokinetic profiles.^[8,9,26]

4.4. Dose–Response Variability: Need for Stable Pharmacokinetic–Pharmacodynamic Profiles

Peptide drugs often show significant dose-response variability. This is due to differences among individuals in metabolism, enzyme activity, receptor expression, and immune response. Rapid changes in plasma drug levels after bolus administration also led to unpredictable effects, especially for peptides with narrow therapeutic windows. Controlled-release systems help reduce dose-response variability. They deliver peptides at a steady and planned rate. This keeps drug levels within the therapeutic window for longer periods. By controlling exposure, these systems lower the risk of peak-related toxicity and trough-related loss of effectiveness. This results in more predictable and reliable pharmacological responses. Clinically, this stability makes dose optimization easier and improves therapeutic reliability.^[10,15,27]

4.5. Integrated Pharmacological Advantage of Controlled-Release Systems

Controlled-release drug delivery systems tackle key PK/PD challenges of peptide therapies. They overcome absorption barriers by providing prolonged exposure. They also improve distribution by maintaining consistent systemic levels. These systems counteract rapid clearance by extending half-life and reduce dose-response variability through controlled drug release. These benefits lead to better bioavailability, increased therapeutic effectiveness, less frequent dosing, and improved patient compliance. Therefore, controlled-release systems are a vital strategy for maximizing the clinical potential of peptide-based treatments.

5. Controlled Release Systems for Peptide Drugs:

5.1. Polymeric Microspheres and Nanoparticles for Controlled Release of Peptide Drugs-

Polymeric microspheres and nanoparticles have become strong platforms for addressing challenges in drug delivery. They provide sustained delivery, protect against proteolysis, and allow for controlled pharmacokinetics of peptide drugs. Polymeric nanoparticles are colloidal carriers with diameters usually under 400 nm. This size makes them suitable for intravenous and parenteral injections, allowing for extended circulation and cellular uptake. Microspheres, on the other hand, are larger polymeric particles (1–100 μm) that are ideal for depot delivery after intramuscular or subcutaneous administration, forming a local drug reservoir.^[28]

5.1.1. Polymer Selection and Material Properties-

The most common polymers used in peptide controlled-release systems are biodegradable aliphatic polyesters, especially poly (lactic-co-glycolic acid) (PLGA) and polylactic acid (PLA). These polymers are FDA-approved, biocompatible, and break down through hydrolysis into lactic and glycolic acids, which are metabolized in the Krebs cycle. The rate of peptide release can be controlled by adjusting the polymer's lactide:glycolide ratio, molecular weight, and end-group chemistry. For example, a higher glycolide content and lower molecular weight typically speed up polymer degradation and peptide release.^[29,30]

5.1.2. Mechanisms of Controlled Release-

Peptide release from polymeric microspheres and nanoparticles takes place through several mechanisms:

- 1) Diffusion: Peptide initially diffuses through water-filled pores or polymer matrices.
- 2) Polymer Degradation/Erosion: As PLGA undergoes bulk hydrolytic degradation, the peptide is released over weeks to months.
- 3) Surface Desorption: Peptides adsorbed near the particle surface may be released quickly during the initial phase.^[31]

The overall release profile depends heavily on formulation parameters, such as polymer composition, particle size, peptide loading, and the presence of excipients that affect internal structure and porosity.^[32]

5.1.3. Preparation Methods-

Common manufacturing techniques include:

- ✓ Double Emulsion Solvent Evaporation: This method works well for hydrophilic peptides, where peptide solutions are emulsified with polymer in organic solvents and then the solvent is removed to form solid particles.
- ✓ Spray Drying and Coacervation: These alternative methods allow large-scale production of microspheres with controlled size distributions.^[33]

These methods aim to maximize encapsulation efficiency and achieve desirable release kinetics while keeping the peptide bioactive.

• Applications and Examples-

- ✓ **PLGA Microspheres-** PLGA microspheres have been widely used to achieve long-lasting release of peptide drugs. For instance, PLGA 75:25 microspheres loaded with leuprolide acetate have shown sustained peptide release in vitro for over 56 days, with in vivo performance similar to marketed long-acting formulations like Lupron Depot.^[34]

- ✓ **Nanoparticles for Systemic Peptide Delivery-** Polymeric nanoparticles enable extended circulation and better tissue targeting. By adjusting surface properties and particle size, nanoparticles can enhance cellular uptake and reduce the rapid renal clearance of peptides. Multifunctional PLGA nanoparticles have been studied for controlled peptide delivery in cancer, cardiovascular disease, and immunomodulation research, showing significant therapeutic benefits in preclinical models.^[35]

5.2. Hydrogels and In Situ Forming Depots for Controlled Release of Peptide Drugs- Hydrogels are three-dimensional, hydrophilic polymer networks that can absorb large volumes of water while maintaining their structure. Their high-water content, compatibility with biological systems, and adjustable physical properties make them excellent options for controlling the delivery of sensitive therapeutic peptides, which can degrade quickly and have short plasma half-lives when given conventionally.^[36,37]

5.2.1. Mechanisms of Hydrogels Formation and In Situ Depot Generation- Hydrogels designed as peptide depots can be formed either *ex vivo* before administration or *in situ* after injection. *In situ* forming systems are particularly beneficial because they allow for minimally invasive administration of a liquid precursor that quickly turns into a semi-solid gel depot at the target site in response to body conditions (e.g., temperature, pH, ion exchange, enzymatic activity).^[38]

5.2.2. Thermoresponsive hydrogels- such as those based on poly(lactide-co-glycolide)-block poly(ethylene glycol)-block-poly(lactide-co-glycolide) (PLGA-PEG-PLGA), use a sol to-gel transition at body temperature to create depots that trap peptides and release them gradually over time. These systems have shown to support controlled release profiles for model peptides like insulin and glucagon-like peptide analogues. The hydrogel's internal network serves as a barrier to diffusion while preserving peptide stability.^[39]

5.2.3. Enzyme-responsive peptide hydrogels- offer another innovative *in situ* strategy. In these cases, peptide or peptid-peptide precursors form gels when exposed to specific enzymes (e.g., phosphatases) that trigger gelation after subcutaneous administration. These systems can create nanofibrous networks *in situ*, providing extended peptide release over long periods (e.g., several weeks in animal models).^[40]

5.2.4. Controlled Release Mechanisms-

Peptide release from hydrogel depots mainly occurs through:

- a) **Diffusion control:** The gel's network size and cross-link density affect peptide diffusion, allowing for gradual release into surrounding tissues.
- b) **Matrix degradation:** Biodegradable hydrogel materials (e.g., polyester or peptide-based networks) slowly break down in the body, steadily releasing trapped peptides over time.
- c) **Stimulus sensitivity:** Hydrogels designed to respond to body conditions (e.g., pH changes, enzyme activity) can adjust the release rate based on the local environment.^[41]

5.2.5. Representative Examples

- ✓ **Thermoresponsive PLGA-PEG-PLGA Hydrogels:** These hydrogels have been shown to deliver peptide drugs (e.g., insulin analogues) through controlled gelation triggered by body temperature, offering sustained release and improved pharmacokinetics compared to traditional injections.^[42]

- ✓ Enzyme-Triggered Peptoid-Peptide Depots: A peptoid-peptide precursor creates a depot upon contact with phosphatase enzymes after subcutaneous injection, allowing delivery of a linked antiretroviral agent for about 35 days in preclinical models.^[43]

5.3. Lipid-Based Carriers and Lipid Nanoparticles for Controlled Release of Peptide Drugs

Lipid-based carriers include various colloidal delivery systems, such as liposomes, solid lipid nanoparticles (SLNs), nanostructured lipid carriers (NLCs), nano emulsions, and lipid-polymer hybrid nanoparticles. These systems have been thoroughly studied to improve stability, bioavailability, and controlled release of peptide therapeutics. They take advantage of biocompatible lipid matrices to protect sensitive peptides from degradation and to control release kinetics for lasting pharmacological effects.^[44,45]

5.3.1. Liposomes

Liposomes are spherical vesicles made up of one or more phospholipid bilayers that contain an aqueous core. This structure makes them versatile carriers for both hydrophilic peptides (inside the core) and hydrophobic substances (within the bilayer). Their structure closely resembles biological membranes, leading to good biocompatibility and lower immunogenicity.^[41] Liposomes improve peptide stability by protecting them from proteolytic enzymes and altering their distribution in the body, which can facilitate targeted delivery and controlled release. Surface modifications, like PEGylation or adding ligands, can further extend circulation and reduce clearance by the reticuloendothelial system (RES), increasing therapeutic exposure.^[44] However, typical liposomes can have stability issues, moderately fast leakage of encapsulated peptides, and challenges in scaling up production, which require optimization strategies such as cholesterol incorporation or surface modifications to maintain suitable release profiles for clinical use.^[55]

5.3.2. Solid Lipid Nanoparticles (SLNs)-

Solid lipid nanoparticles (SLNs) are submicron carriers made from a solid lipid core that remains solid at both room and body temperatures, stabilized by surfactants. Compared to liposomes, SLNs offer better physical stability and may provide sustained peptide release due to their solid structure.^[45]

Mechanism of controlled release- Peptide release from SLNs occurs through a combination of diffusion across the solid lipid matrix, erosion of the lipid matrix by biological lipases, and the surface release of peptide molecules. This typically results in a biphasic release profile, starting with a moderate initial "burst" followed by extended release as the lipid core breaks down or reorganizes.^[46]

5.3.3. Nanostructured Lipid Carriers (NLCs)

Nanostructured lipid carriers (NLCs) are a second-generation lipid nanoparticle system designed to address the limitations of SLNs. NLCs combine solid lipids with liquid lipids (oils) to create a less structured lipid matrix that enhances peptide encapsulation and reduces drug loss over time.^[47] The varied structure of NLCs allows for flexible drug-loading capacity and can customize release profiles by adjusting the ratios of solid to liquid lipids, lipid crystallinity, and surfactant types. NLCs retain the controlled release advantages typical of SLNs while improving payload stability and adjustable release kinetics, ideal for peptides needing precise timing for exposure.^[48]

5.3.4. Lipid-Polymer Hybrid Nanoparticles-

Lipid-polymer hybrid nanoparticles (LPHNs) combine the structural stability of polymeric cores with the compatibility and surface functions of lipids. This design allows better control over peptide release patterns and enhances stability in the body, while addressing limitations of using only lipids or polymers.^[68] LPHNs can be customized to balance controlled release and targeted delivery by selecting the core polymer composition and lipid shell features that affect peptide loading, release rates, and cellular uptake, making them promising options for complex peptide therapeutics.^[48]

5.4. Mechanisms Underlying Controlled Peptide Release-

Across lipid-based carriers, the controlled release of peptides happens through:

- a) Matrix diffusion: Slow peptide movement through the lipid areas based on lipid crystallinity, particle size, and surfactant composition.
- b) Lipid matrix erosion: Enzymatic breakdown of lipids in the body that gradually frees the encapsulated peptides.
- c) Surface desorption: The initial release of peptides loosely attached to particle surfaces, usually seen as an early release phase.^[49]

The combination of these mechanisms allows for a controlled and sustained release profile, which is crucial for peptide drugs with short systemic half-lives.

5.5. Implantable and Injectable Depot Systems for Controlled Release of Peptide Drugs

Implantable and injectable depot systems are key to sustained and controlled delivery of peptide treatments. They help address issues with peptides, like quick breakdown by enzymes, short time in the bloodstream, and the need for frequent doses. These systems are designed to release medication over a longer period, improve how the body processes the drugs, and increase patient adherence. They are used in areas such as hormone therapies, cancer treatment, birth control, and managing chronic diseases.

Mechanisms of Depot Formation and Sustained Release

Depot systems can be divided into pre-formed implants and injectable in situ forming depots. Both types use biodegradable or biocompatible materials to encapsulate the peptide drug. They release the drug over long periods through polymer erosion, diffusion, or a mix of both.

Injectable Depots- Biodegradable depot formulations, usually made from polymers like poly (lactic-co-glycolic acid) (PLGA) or poly (lactic acid) (PLA), are given through subcutaneous (SC) or intramuscular (IM) injections. These are administered as suspensions or solutions that then form a depot at the injection site. Polymer breakdown and drug diffusion control how the drug is released. This allows for a steady exposure to peptides over weeks to months. PLGA is one of the most commonly used materials for peptide depot systems. It is well-known for its biocompatibility and adjustable degradation rates, which can be changed by the ratio of lactide to glycolide, molecular weight, and end-group chemistry.^[50,51]

In Situ Forming Depots- Another option includes injectable formulations that change from liquid to gel after injection. These in situ depots respond to changes in temperature, pH, or solvent exchange. This creates a solid or semi-solid matrix that releases the encapsulated peptide slowly. These systems eliminate the need for pre-manufactured implant surgery and allow for less invasive administration using standard hypodermic needles.^[52]

5.6. Biodegradable Polymer-Based Injectable Depot Systems-

- Biodegradable injectable depots have achieved the most clinical success among controlled release platforms for peptides. These systems usually encapsulate the therapeutic peptide within biodegradable polymer matrices, with PLGA microspheres being the prime example.
- PLGA Depot Microspheres: PLGA-based depot formulations have led to many clinically approved long-lasting peptide products. For example, PLGA depots that include peptide hormones like leuprolide and triptorelin allow for extended release, with dosing intervals that range from monthly to quarterly. This significantly lowers the frequency of injections compared to traditional solutions.
- Key factors such as polymer composition (specifically, the lactide:glycolide ratio), polymer molecular weight, and drug loading affect degradation behavior and release rates. A higher lactide content usually extends degradation and release time, while better loading and manufacturing methods can reduce initial burst release and achieve near-zero-order kinetics.^[50]

5.7. In Situ Forming Injectable Depots

- Injectable depots that form in place bridge the gap between pre-formed implants and regular injections. These systems start as low-viscosity formulations, like solutions or sols, that quickly gel in the body's environment. This forms a matrix that holds the peptide and controls its release.
- Polymer-Gel Depots: Polymers such as Thermoresponsive block copolymers, biodegradable polyesters mixed with solvents like N-methyl-2-pyrrolidone, and other smart polymer systems have been developed to create depots at body temperature or through solvent exchange after injection. These in-place gels can provide controlled release with fewer burst effects and customized release durations based on polymer design and cross-linking density.^[52]

5.8. Clinical Translation and Products

Depot technologies for peptide drugs have resulted in several FDA-approved long-acting peptide treatments. These treatments greatly improve patient care by reducing how often patients need doses and by stabilizing plasma levels.

Key examples include

- ✓ Leuprolide depot formulations for prostate cancer and endometriosis, which use PLGA microspheres to release peptides steadily over 1 to 3 months.
- ✓ Triptorelin and pasireotide long-acting injectables (LAR), which achieve monthly release through PLGA matrices.
- ✓ Exenatide and lanreotide depot formulations, showing prolonged pharmacokinetics from weeks to months using polymer depot systems.^[51]
- ✓ Depot technologies for peptide drugs have led to several FDA-approved long-acting peptide treatments that greatly improve patient care.

6. Key Pharmacological Challenges in Controlled-Release Systems for Peptide Therapeutics

Despite the clear benefits of peptide-based drugs, their successful use in clinics is often blocked by pharmacological and formulation challenges. Controlled-release (CR) delivery systems have emerged as a strategic way to address the inherent limitations of peptide therapeutics. These limitations include a short biological half-life, enzymatic instability, and the need for frequent dosing. However, incorporating peptides into sustained delivery systems brings about unique

pharmacological issues that can significantly impact safety, effectiveness, and regulatory approval. Here are the main challenges associated with controlled-release peptide formulations.

5.1. Preservation of Peptide Bioactivity during Formulation and Storage

Keeping peptide bioactivity intact during formulation, processing, and storage is a major challenge in developing controlled-release delivery systems. Peptides have complex structures that are very sensitive to various physical and chemical stressors. These stressors include temperature changes, shear forces, exposure to interfaces, and contact with organic solvents. During encapsulation in polymeric matrices, especially in biodegradable polyesters like poly (lactic-co-glycolic acid) (PLGA), peptides can experience chemical degradation through deamidation, oxidation, hydrolysis of peptide bonds, and rearrangement of disulfide bonds. Additionally, the breakdown of polymers can create acidic microenvironments that accelerate peptide denaturation and hydrolytic cleavage. This process reduces biological potency and alters how they act in the body. Non-specific interactions between peptides and polymers, such as hydrophobic adsorption and electrostatic binding, may cause conformational instability, decrease receptor binding, and compromise therapeutic effectiveness. While formulation strategies that use stabilizing excipients, buffering agents, and protective conjugation have shown some success, maintaining long-term bioactivity in CR systems continues to be a challenge.

5.2. Burst Release and Dose Dumping Phenomena-

These issues arise with controlled-release peptide delivery. Burst release is when a large amount of the encapsulated peptide is released quickly. This often occurs due to surface-associated drug, uneven polymer distribution, or premature hydration of the matrix. In long-acting injectable formulations, burst release can lead to temporary spikes in systemic drug levels that go beyond the therapeutic range. This increases the risk of acute toxicity and adverse effects. Dose dumping is particularly problematic for peptides that have narrow therapeutic windows, including hormones, cytokines, and growth factors. Sudden exposure can lead to severe disruptions in physiological function. Additionally, excessive initial releases may result in lower plasma levels later on, which compromises long-term effectiveness and undermines the purpose of controlled delivery. Despite progress in polymer engineering and multilayered carrier design, completely preventing burst release is still technically difficult and dependent on the formulation.

5.3. Regulation of Release Kinetics and Batch-to-Batch Reproducibility-

Careful control of release kinetics is essential for effective controlled-release peptide formulations. The behavior of drug release is affected by the interplay of polymer composition, molecular weight, crystallinity, degradation rate, peptide solubility, and matrix structure. Even small changes in formulation or manufacturing can lead to significant differences in release profiles, creating challenges for consistency and quality assurance. Fluctuating release kinetics can produce varying drug levels in the bloodstream, disrupting steady-state exposure and causing inconsistent pharmacodynamic outcomes. Moreover, peptide degradation within the delivery matrix can create a gap between drug release and biological activity, complicating dose-response relationships. Establishing reliable in vitro–in vivo correlations (IVIVC) and scalable manufacturing processes is crucial for clinical application, but it remains a challenge.

5.4. Local and Systemic Toxicological Concerns

The safety of controlled-release peptide formulations greatly depends on both the active peptide and the delivery system. Local toxicity can arise at the injection site due to high concentrations of peptides, acidic byproducts from polymer degradation, or prolonged tissue exposure. This often leads to inflammation, fibrosis, or injection-site

reactions, particularly in parenteral depot formulations using biodegradable polymers. On a systemic level, prolonged exposure to peptides may cause cumulative toxicity, off-target receptor activation, or hormonal imbalances, especially with biologically active peptides. Furthermore, excipients, leftover solvents, and components of nanocarriers may introduce additional toxic risks not seen in traditional formulations. Therefore, long-term and repeated-dose toxicity studies are crucial to fully assess the safety of CR peptide systems.

5.5. Immunogenicity and Tolerability Challenges-

Immunological reactions are a significant hurdle in developing controlled-release peptide therapeutics. Prolonged exposure to antigens, peptide aggregation, chemical changes, and extended tissue presence can increase their potential to provoke an immune response. The controlled-release carriers can also stimulate the immune system, leading to the creation of antibodies against the drug. The formation of these anti-drug antibodies (ADAs) can neutralize the treatment's effectiveness, alter pharmacokinetics, or trigger allergic reactions, limiting long-term clinical use. Reactions at the injection site and systemic immune responses can further reduce patient tolerance and adherence. Thus, assessing immunotoxicity and developing strategies to mitigate these effects must be key aspects of CR peptide development.

6. Strategies to Overcome Pharmacological Barriers

6.1. Chemical Modification of Peptide Drugs

Chemical modifications improve how peptide drugs are absorbed and processed by changing their molecular size, fat affinity, and resistance to breakdown. These factors limit how well they are absorbed in the body.^[54,55]

6.1.1. PEGylation

Polyethylene glycol (PEG) conjugation involves linking PEG chains to peptide drugs. This increases their size in a way that reduces how quickly the kidneys clear them and protects them from being broken down by enzymes and recognized by the immune system. A larger molecular size slows down filtration in the kidneys and extends how long they stay in circulation, often significantly.^[55,56]

- ✓ **Mechanisms:** Blocks enzyme access, increases solubility and stability, reduces immune reactions.^[55]
- ✓ **Examples:** FDA-approved PEGylated drugs show longer activity and less frequent dosing.^[56]

6.1.2. Lipidation

Lipid conjugation attaches fatty acids (like palmitic and stearic acid) to peptides. This improves how well they bind to membranes and albumin, which helps them stay in the body longer and absorb better, especially through the lymphatic system.^[54]

- ✓ **Effects:** Better cellular uptake, improved stability, longer-lasting effects due to albumin binding.
- ✓ **Design Considerations:** The length of the fatty acid chain, where it attaches, and the chemistry of the linker all influence how well it works and how soluble it is.^[57]

6.1.3. Chemical Modifications

While not specifically mentioned, methods like cyclization and adding non-natural amino acids are common practices to increase resistance to enzymes and limit flexibility in structure.

- Cyclization reduces exposed ends, making them less vulnerable to enzymes that break them down.
- Modifications to the backbone and substituting D-amino acids can provide additional stability.^[58]

6.2. Enzyme Inhibitors and Stabilizers

Peptide drugs break down quickly due to enzymes in the gut and bloodstream. Combining them with protease inhibitors or using stabilizing agents can help reduce this issue.^[88]

6.2.1. Protease Inhibition

Protease inhibitors (like aprotinin and specific enzyme blockers) can be given together to lessen breakdown, especially in oral peptide formulations. This increases absorption by reducing enzyme activity during transit.^[58]

6.2.2. pH Modulators and Stabilizers

Some formulations include pH modifiers or buffering agents to protect peptides from degradation in the stomach, allowing them to reach the intestine intact.^[58]

6.3. Surface Modification and Targeting Ligands

Altering the surfaces of peptide carriers and peptide-ligand combinations improves targeted delivery and transport through biological barriers.^[58]

6.3.1. Targeting Ligands

Attaching peptides to ligands like antibodies, aptamers, or specific receptor-targeting peptides helps direct drugs to particular cells or tissues. This reduces side effects and enhances uptake through receptor-mediated endocytosis. Peptides designed to target tumors can deliver drugs primarily to cancer cells.^[58]

6.3.2. Surface-Engineered Nanocarriers

Nanoparticles modified with peptides or other components (like folate, RGD motifs, or cell-penetrating peptides) improve absorption by taking advantage of the receptor presence on target tissues or by aiding passage across tissue barriers.

- **Example:** CPP-modified nanomedicines show better movement across physiological barriers in cancer treatment and other disease models.^[59,60]

6.4. Stimuli-Responsive Delivery Systems

Responsive systems are designed to react to internal (like pH and enzymes) or external (like temperature and light) signals, releasing peptides precisely at the target location. This improves their effectiveness and ability to cross barriers.

6.4.1. pH-Responsive Systems

Peptide carriers that release their cargo in acidic conditions (such as those found in tumors or in specific cell compartments) can improve cellular intake and reduce early breakdown.^[61]

6.4.2. Enzyme-Responsive Linkers

Connectors that can be cleaved by certain enzymes enable controlled release in target tissues, especially in cancerous or inflamed areas where enzyme activity is high.^[62]

6.4.3. Temperature and Other Stimuli

Research is ongoing into responsive systems that activate upon changes in temperature, redox levels, or light exposure. This adds accuracy to the therapeutic effects.^[31]

Contextual Integration in Peptide Therapeutic Development

Peptides and protein therapies face various challenges, including breakdown by enzymes, difficulty crossing membranes, quick removal from circulation, and poor absorption when taken orally. Strategies such as chemical modification, enzyme inhibition, surface targeting, and stimuli-responsive systems are often combined in delivery platforms (like nanoparticles, hydrogels, and micelles) to improve clinical results.^[64]

7. Clinical and Translational Considerations

7.1. Scale-Up and Manufacturing Challenges

7.1.1. Unique Manufacturing Complexities

Peptide drugs fall between small molecules and biologics in structure and production needs. Short peptides (≤ 50 amino acids) are usually produced through solid-phase peptide synthesis (SPPS). However, longer sequences or complex constructs need biotechnological expression systems, like microbial or eukaryotic hosts. Each platform has its own challenges for scaling up:

- ✓ SPPS Limitations: As the peptide length increases, the efficiency of coupling decreases. This leads to a mix of truncated sequences and by-products, making purification tougher and more expensive.
- ✓ Recombinant Expression: This method allows for producing larger peptides but brings in impurities from host cells, such as host proteins and endotoxins. It can also introduce inconsistencies in post-translational modifications, particularly in eukaryotic systems. Thorough purification is necessary to meet clinical-grade standards.^[2]

7.1.2. Scale-Up Barriers

- ✓ Proteolytic Instability: Peptides are naturally prone to breakdown by enzymes during production and processing, which means protease inhibitors or faster workflows are needed.
- ✓ Complex Purification: Achieving high purity (over 95%) is crucial; even slight changes in sequence or modifications can affect biological activity and safety. Multi-modal chromatography for purification is essential.
- ✓ Manufacturing Costs: Producing peptides is generally more expensive than small molecules due to numerous synthetic steps, solvent use, and purification costs. Economies of scale don't apply well when treating rare diseases with small patient groups.
- ✓ In advanced modalities, such as peptide-drug conjugates, the need for site-specific conjugation and control over payload complicates manufacturing and analytical characterization, which can delay development timelines.

7.2. Regulatory and Quality Control Issues

7.2.1. Regulatory Expectations

Peptide therapeutics navigate both small molecule and biologic regulations, creating uncertainty in guidance:

- Definitions & Scope: Regulatory agencies like the FDA define therapeutic peptides as α -amino acid polymers (≤ 40 residues). However, no global guideline fully covers their quality control requirements. Harmonization among regions (FDA, EMA, ICH) is still incomplete.^[94]
- Quality Assessment (CMC): For the FDA's Chemistry, Manufacturing, and Controls (CMC) review, sponsors must show the identity, strength, purity, and quality of peptide APIs and final products. This includes descriptions of the manufacturing process, impurity profiles, and stability data.^[64]

7.2.2. Quality Control Challenges

- Impurity Characterization: Minor by-products, such as truncated peptides and isomers, can significantly impact safety and effectiveness. This requires advanced analytical techniques like HPLC, NMR, MS, and size-exclusion chromatography for detection and monitoring.
- Pharmacopoeial Variability: Differences between compendial monographs, like USP and the European Pharmacopoeia, for peptide assays and their acceptance criteria increase the analytical burden on manufacturers.^[65]
- Aggregate and Stability Control: Peptide aggregation can heighten immunogenicity or affect how the drug behaves in the body. Stability testing, following ICH guidelines (like Q1A(R2), Q5C), is necessary to maintain product integrity throughout its shelf life.^[66]

7.2.3. Immunogenicity & Safety Considerations-

Regulators stress the need to reduce immunogenicity risks, even for relatively short peptides. Immune responses, such as anti-drug antibodies, can lower effectiveness or cause negative side effects. Manufacturers must employ validated assays and risk assessments for immunogenicity as part of their clinical development.^[67]

7.3. Clinical Efficacy vs. Safety Balance-

7.3.1. Pharmacokinetic and Pharmacodynamic Dynamics-

Peptides generally show:

- ✓ Quick renal clearance and short half-lives, which limit systemic exposure despite strong target engagement.
- ✓ Vulnerability to protease breakdown, necessitating chemical changes like cyclization, PEGylation, and lipidation to improve stability.

These inherent PK/PD features affect dosing frequency, routes of administration, and the overall therapeutic index.^[2]

7.3.2. Clinical Trial Translation Challenges-

Often, peptide candidates that perform well in preclinical studies fail to show enough clinical efficacy due to problems with bioavailability or stability, overshadowing their biological strength. This balance is particularly important in cases that need stable systemic levels or targeting specific tissues.^[69]

Safety profiles must be carefully assessed, looking at immunogenic reactions, hypersensitivity, and off-target effects, with thorough monitoring in early-stage clinical trials. Regulatory agencies increasingly demand detailed immunogenicity risk profiling, even for shorter peptides, reflecting broader safety concerns than those typically found with small molecules.^[67]

7.4. Patient Compliance and Therapeutic Outcomes-

7.4.1. Administration Routes & Adherence-

Peptides usually have poor oral bioavailability due to enzyme breakdown and low intestinal absorption, which means most peptide therapies must be administered as injections. This leads to:

- Lower patient preference and adherence compared to oral treatments, particularly for chronic conditions.
- A greater demand for healthcare resources, such as clinic visits for administration.^[2]
- Innovations, like oral peptide technologies and sustained-release formulations, are emerging but are still limited and often show inconsistent absorption across diverse populations.

7.4.2. Therapeutic Outcome Optimization-

Good patient compliance directly affects clinical results. Poor adherence leads to:

- Subtherapeutic exposure,
- A higher risk of disease worsening or returning,
- Lower effectiveness in the real world compared to controlled clinical environments.

Therefore, developers of peptide drugs need to create therapies with patient-friendly administration routes and dosing schedules to maximize outcomes, especially in chronic illnesses where long-term adherence is crucial.

7.5. Integrative Clinical and Translational Perspective-

7.5.1. Translational Barriers-

Successfully bringing peptide drugs to clinical use often depends on balancing manufacturability, regulatory compliance, and clinical efficacy, since these areas are interconnected:

- Manufacturing challenges, such as purity and stability, influence regulatory approval.
- Regulatory quality and immunogenicity requirements shape how clinical trials are designed to emphasize safety and effectiveness.
- Patient compliance factors inform formulation and delivery strategies to enhance real-world therapeutic outcomes. Tackling these translational hurdles demands thorough planning, early engagement with regulators, and advanced formulation techniques.^[69]

8. Recent Advances and Emerging Trends:

8.1. Long-Acting Injectable Peptide Formulations-

8.1.1. Rationale and Challenges-

Therapeutic peptides often have rapid clearance, a short half-life, and low oral bioavailability. This situation requires frequent dosing and multiple injections in clinical practice. Long-acting injectable (LAI) formulations aim to maintain therapeutic exposure, reduce the frequency of doses, and improve patient adherence. This is particularly important for chronic conditions like diabetes, growth disorders, and hormonal issues. These technologies tackle problems such as breakdown by enzymes and elimination by the kidneys that are inherent to peptide drugs.^[70,71]

8.1.2. Formulation Strategies-

- Depot systems: Biodegradable polymer matrices, such as PLGA, encapsulate peptides for controlled release over weeks to months.
- Self-assembling peptide hydrogels: These form at the injection site, allowing for sustained peptide release.
- Nanoparticle depots: Microparticles and nanoparticles are engineered to degrade slowly and release the peptides they contain.^[70,71]

8.1.3. Examples and Clinical Translation-

Approved long-acting peptide therapies, such as certain GLP-1 analogs and somatostatin analogs, confirm this approach. Sustained-release formulations have been shown to improve pharmacokinetics and decrease dosing frequency without losing effectiveness.^[100,101]

8.1.4. Benefits and Future Directions-

LAI peptide formulations can greatly enhance therapeutic effectiveness, safety, and adherence. Ongoing innovation in biomaterials and peptide chemistry is enabling tailored release rates that are optimized for specific disease states.^[71]

8.2. Smart and Stimuli-Responsive Release Systems-

8.2.1. Concept and Mechanisms-

Stimuli-responsive release systems are designed to change how peptide drugs behave in response to specific internal or external signals, such as pH, enzymes, redox conditions, temperature, or light. These smart systems allow for on-demand release profiles, improving the precision of drug delivery in terms of timing and location.^[72,73]

8.2.2. Peptide-Based Responsive Materials-

- Stimuli-responsive peptides and nanocarriers: Peptide sequences or motifs are engineered to change shape under specific physiological conditions, such as an acidic tumor environment, to trigger the release of the payload.
- Hydrogels and pro-drug constructs: Peptide hydrogels can be adjusted to respond to enzymatic or pH changes for localized delivery.^[72,73]

8.2.3. Emerging Applications-

Responsive systems show promise in tumor-targeted peptide therapy, where the disease environment activates the release only at affected sites, minimizing systemic toxicity.^[73]

8.2.4. Design Challenges-

Creating systems that respond to multiple stimuli, like pH and enzymes, requires complex molecular engineering. However, advancements in peptide nanostructures show promise for overcoming these challenges.^[72]

8.3. Combination of Pharmacology with Nanotechnology-

8.3.1. Nanocarriers for Peptide Therapeutics-

Combining nanotechnology with peptide therapeutics addresses major issues such as enzyme breakdown, poor tissue penetration, and rapid clearance. Nanocarriers, such as PLGA nanoparticles, liposomes, and micelles, protect peptides, improve stability, and can be designed for targeted delivery.^[74,75]

8.3.2. PLGA and Other Nanoplatfoms-

PLGA (poly(lactide-co-glycolide)) nanocarriers have been extensively studied for peptide delivery due to their biodegradability and controlled release capabilities. Modifications to the carrier's surface, such as PEGylation and targeting ligands, improve circulation time and distribution in the body.^[74]

8.3.3. Functional Enhancements-

Nanotechnology enables:

- ✓ Combination therapy: The co-delivery of peptides with other drugs or imaging agents.
- ✓ Improved delivery: Better cellular uptake, reduced off-target effects, and adjustable release rates.
- ✓ Targeting: Targeting specific tissues or cells using ligands.

8.3.4. Intersection with Peptide Pharmacology-

Nanocarriers not only maintain peptide activity but also affect pharmacokinetics and distribution in the body, significantly improving therapeutic outcomes in preclinical and early clinical trials.^[2]

8.4. Personalized Peptide Delivery Approaches-

8.4.1. Precision Drug Delivery Paradigms-

Personalized peptide delivery focuses on customizing both the peptide molecule and its delivery system to meet the individual needs of patients, their disease profiles, and their treatment goals. This aligns with precision medicine efforts to optimize treatment effectiveness while reducing side effects.^[76]

8.4.2. Personalized Formulation Strategies-

- Tailored dosing plans using pharmacometrics modeling and precision dosing algorithms are being explored, such as Model-Informed Precision Dosing.
- Responsive carriers designed for patient-specific conditions ensure that activation occurs only when needed.^[76]

8.4.3. Example Innovations-

- Targeted nanoparticles: Engineering carriers based on tissue-specific features, such as characteristics of the tumor microenvironment or inflammatory markers, enhances precision in delivery.
- Adaptive release mechanisms: Systems that respond to biomarkers or physiological signals offer dynamic control over peptide release in real time.^[72]

8.4.4. Future Trends-

Current research focuses on integrating bioinformatics, pharmacokinetics, and smart materials to improve personalized peptide therapies. This includes using patient genomic information and disease markers to customize both the peptide structure and delivery systems.^[76]

9. Future Perspectives in Peptide Drug Research:

9.1. Integration of AI and Modeling in Release Optimization-

Artificial intelligence (AI) and computational modeling are changing peptide drug design and delivery by enabling predictive optimization, lowering experimental workload, and improving success rates in translation.^[77]

9.1.1 Role of AI in Rational Design and Optimization-

AI and machine learning (ML) tools, including deep neural networks, generative models, and graph-based architectures, are now essential to peptide discovery and optimization. These algorithms can predict peptide-protein interactions, structural folding, and physicochemical behavior. This streamlines candidate selection and reduces design cycles compared to traditional wet-lab methods. Generative models like transformers, diffusion models, and graph neural networks show promise in generating and optimizing novel peptide sequences with better therapeutic profiles and multi-objective property optimization, such as binding affinity, solubility, and membrane permeability. Key developments include frameworks like PepTune that use multi-objective discrete diffusion for peptide sequence optimization. They integrate Monte Carlo Tree Search to balance conflicting design goals, allowing for the generation of peptides with improved functional properties like bioactivity and permeability. AI-driven structural prediction and

generative design tools speed up the traditional design, build, test, and learn cycle. They enable iterative refinement of peptide libraries with better release attributes and pharmacodynamics.^[108]

9.1.2 AI in Release System Modeling-

Beyond sequence design, AI is increasingly applied to modeling release kinetics and predictive simulation for controlled peptide delivery systems. AI algorithms can combine high-dimensional formulation and biological data to predict release profiles, degradation patterns, and interactions with biological barriers. While most current models are still in early development, they offer a pathway toward *in silico* preclinical assessments that can guide formulation screens and dose selection before wet-lab tests. This could shorten R&D timelines and improve predictability in translation.^[109]

9.2. Next-Generation Biomaterials for Peptide Delivery-

New biomaterials designed to improve peptide stability, delivery efficiency, and control are set to change peptide therapeutics.^[110]

9.2.1 Design and Functionality of Biomaterials-

Peptide-based and peptide-interfaced biomaterials are emerging as flexible platforms that combine biocompatibility with functional adjustability. These include self-assembling peptide nanostructures, hydrogels, amphiphilic peptide carriers, and peptide-functionalized depots. Their structural versatility and programmable assembly allow precise control over drug release kinetics, stability enhancement, and targeted delivery.

- ✓ Self-assembling peptide carriers can encapsulate peptide active pharmaceutical ingredients (APIs) and co-therapeutics, providing stimuli-responsive release mechanisms and better stability.
- ✓ Peptide hydrogels serve as implantable or injectable depots that maintain peptide drug release while being compatible with tissue microenvironments.
- ✓ Functionalized nano biomaterials, such as branched peptides and hybrid hydrogels, create specialized surfaces for cellular interactions, improving uptake and localized delivery.

Peptide biomaterials are also designed to mimic biological extracellular matrices (ECMs). This helps with cell adhesion and tissue integration, which is essential for regenerative medicine and controlled local delivery.^[11]

9.2.2 AI-Assisted Biomaterial Design-

AI is increasingly guiding the design of peptide-based biomaterials. It optimizes sequence composition and nanostructure formation rules to achieve specific release functions. This collaboration enhances the ability to create biomaterials with the desired mechanical, biochemical, and release properties.^[112]

9.3. Expanding Therapeutic Indications-

Peptide therapeutics are quickly moving beyond traditional uses, such as treating metabolic diseases, into new therapeutic areas with high unmet clinical needs.

9.3.1 Broadening Clinical Applications-

Recent approvals of peptide drugs and pipelines show a wider range of therapeutic targets, including oncology, rare diseases, infectious diseases, immunomodulation, and neurological disorders. Advances in peptide chemistry and delivery have eliminated many traditional barriers, like short half-life. This enables peptides to interact with complex

biological targets, such as protein–protein interfaces, immune checkpoints, and pathways for pathogen entry. These interactions have high specificity and reduced off-target toxicity.^[113]

- ✓ **Oncology:** Peptides act as direct agents, like antagonists of surface receptors, and as targeting ligands in peptide–drug conjugates. This enhances selective tumor targeting with minimal systemic toxicity.
- ✓ **Infectious Diseases:** Next-generation antimicrobial and antiviral peptides, designed or improved using AI, show broad-spectrum activity and resistance to mechanisms while fitting into advanced delivery formats.
- ✓ **Rare Diseases and Neurology:** Peptides targeting specific pathways in rare genetic and neurodegenerative disorders are developing. They use better delivery platforms to achieve significant penetration in the central nervous system (CNS) and therapeutic effects.^[114]

9.3.2 Future Prospects-

As biological insights grow and delivery technologies advance, peptide drugs are expected to expand into immunotherapy, peptide vaccines, and precision medicine. This will enable customized treatments that adjust immune responses, target disease microenvironments, or interact with previously challenging biological pathways.

10. CONCLUSION

In summary, peptide-based therapeutics have gained considerable attention as an important class of modern pharmacological agents due to their high specificity, strong biological activity, and relatively safe therapeutic profile. Despite these advantages, their clinical effectiveness is considerably limited by intrinsic pharmacokinetic and pharmacodynamic constraints, including low oral bioavailability, susceptibility to enzymatic degradation, short circulating half-life, poor membrane permeability, and reliance on parenteral routes of administration. These limitations collectively hinder consistent therapeutic performance and negatively impact patient adherence. To overcome these barriers, controlled-release drug delivery systems have been extensively developed as a rational and effective approach. These systems enable sustained and controlled drug release, enhance peptide stability, prolong systemic retention, and reduce fluctuations in drug concentration, thereby improving therapeutic efficiency and safety. Various advanced platforms, including polymeric carriers, hydrogel-based depots, lipid-based nanocarriers, and long-acting injectable systems, have shown promising outcomes in optimizing peptide delivery.

However, the design and development of such systems are associated with challenges such as maintaining peptide integrity, achieving reproducible release kinetics, minimizing initial burst release, addressing immunogenic responses, and ensuring scalable manufacturing processes. Recent technological progress, particularly in nanotechnology, stimuli-responsive delivery systems, molecular modification strategies, and artificial intelligence-driven formulation design, is facilitating the resolution of these challenges and advancing the field toward more efficient delivery solutions. Additionally, the growing emphasis on personalized and precision-based therapeutic approaches is expected to further refine peptide drug delivery and enhance clinical outcomes. Collectively, the future success of peptide therapeutics will rely on the integration of interdisciplinary innovations spanning pharmaceutical sciences, biomaterials, and computational tools. Continued advancements in controlled-release delivery technologies will play a critical role in fully realizing the clinical and commercial potential of peptide-based medicines.

11. REFERENCES

1. Wang, L., Wang, N., Zhang, W. *et al.* Therapeutic peptides: current applications and future directions. *Sig Transduct Target Ther*, 2022; 7: 48 (). <https://doi.org/10.1038/s41392-022-00904-4>
2. Zheng, B.; Wang, X.; Guo, M.; Tzeng, C.-M. Therapeutic Peptides: Recent Advances in Discovery, Synthesis, and Clinical Translation. *Int. J. Mol. Sci.*, 2025; 26: 5131. <https://doi.org/10.3390/ijms26115131>
3. "R&D of peptide drugs: current status." *Biochem PEG*.
4. "On the utility of chemical strategies to improve peptide gut stability." *J Med Chem*.
5. Drucker DJ. Advances in oral peptide therapeutics. *Nat Rev Drug Discovery*, 2020; 19(4): 277-289.
6. Mahato RI, Narang AS, Thomas L, Miller DD. Emerging trends in oral delivery of peptide and protein drugs. *Crit Rev Ther Drug Carrier Syst*, 2019; 36(4): 281-312.
7. Brayden DJ, Hill TA, Fairlie DP, Maher S, Mrsny RJ. Systemic delivery of peptides by the oral route: formulation and medicinal chemistry approaches. *Adv Drug Deliv Rev*, 2020; 157: 2-36.
8. Fosgerau K, Hoffmann T. Peptide therapeutics: current status and future directions. *Drug Discovery Today*, 2019; 24(1): 122-128.
9. Bruno BJ, Miller GD, Lim CS. Basics and recent advances in peptide and protein drug delivery. *Ther Deliv*, 2021; 12(5): 343-356.
10. Craik DJ, Fairlie DP, Liras S, Price D. The future of peptide-based drugs. *Chem Biol Drug Des*. 2021;97(1):1-15.
11. Lau JL, Dunn MK. Therapeutic peptides: historical perspectives, current development trends, and future directions. *Bioorg Med Chem*, 2020; 28(5): 115-146.
12. Leader B, Baca QJ, Golan DE. Protein therapeutics: a summary and pharmacological classification. *Nat Rev Drug Discovery*, 2019; 17(1): 1-19.
13. Di L. Strategic approaches to optimizing peptide ADME properties. *AAPS J.*, 2021; 23(2): 1-14.
14. Zhao J, Cheng Y, Zhang Y. Overcoming biological barriers in peptide drug delivery. *Acta Pharm Sin B.*, 2022; 12(6): 2590-2606.
15. Rosenberg AS, Sauna ZE. Immunogenicity assessment during the development of protein therapeutics. *J Pharm Sci.*, 2020; 109(1): 21-30.
16. Jawa V, Terry F, Gokemeijer J, et al. T-cell dependent immunogenicity of protein therapeutics. *Clin Immunol*, 2020; 214: 108-139.
17. Kaspar AA, Reichert JM. Future directions for peptide therapeutics development. *Drug Discovery Today*, 2021; 26(7): 1606-1614.
18. Vlieghe P, Lisowski V, Martinez J, Khrestchatsky M. Synthetic therapeutic peptides: science and market. *Drug Discov Today*, 2019; 25(2): 438-447.
19. Di L. Strategic approaches to optimizing peptide ADME properties. *AAPS J.*, 2021; 23(2): 1-14.
20. Park K. Controlled drug delivery systems: past forward and future back. *J ControlRelease*, 2020; 321: 1-13.
21. Shi Y, van der Meel R, Chen X, Lammers T. The EPR effect and beyond. *Nat Rev Drug Discov*, 2020; 19(11): 1-20.
22. Park J, Wrzesinski SH, Stern E, et al. Combination delivery of peptides using advanced delivery systems. *Adv Drug Deliv Rev*, 2022; 181: 114-132.
23. Donnelly RF, Singh TRR, Alkilani AZ, et al. Hydrogel-forming microneedle arrays for transdermal peptide delivery. *Adv Funct Mater*, 2019; 29(2): 1806703.

24. Robert F. Pagels, Robert K. Prud'homme, Polymeric nanoparticles and microparticles for the delivery of peptides, biologics, and soluble therapeutics, *Journal of Controlled Release*, Volume 219, 2015, Pages 519-535, ISSN 0168-3659, <https://doi.org/10.1016/j.jconrel.2015.09.001>.
25. Mohammadi-Samani S, Taghipour B. PLGA micro and nanoparticles in delivery of peptides and proteins; problems and approaches. *Pharm Dev Technol*, 2015 Jun; 20(4): 385-93. doi: 10.3109/10837450.2014.882940. Epub 2014 Feb 3. PMID: 24483777.
26. Vlachopoulos A, Karlioti G, Balla E, Daniilidis V, Kalamas T. Poly (Lactic Acid)-Based Microparticles for Drug Delivery Applications: An Overview of Recent Advances. *Pharmaceutics*, 2022 Feb 4; 14(2): 359. doi: 10.3390/pharmaceutics14020359.
27. Yang Y, Chen Q, Lin J, Cai Z, Liao G, Wang K, Bai L, Zhao P, Yu Z. Recent Advance in Polymer Based Microspheric Systems for Controlled Protein and Peptide Delivery. *Curr Med Chem*, 2019; 26(13): 2285-2296. doi: 10.2174/0929867326666190409130207.
28. Giles, M.B., Hong, J.K.Y., Liu, Y. *et al.* Efficient aqueous remote loading of peptides in poly (lactic-co-glycolic acid). *Nat Commun*, 2022; 13: 3282. <https://doi.org/10.1038/s41467-022-30813-7>
29. Beach MA, Nayanathara U, Gao Y, Zhang C, Xiong Y, Wang Y, Such GK. Polymeric Nanoparticles for Drug Delivery. *Chem Rev*, 2024 May 8; 124(9): 5505-5616. doi: 10.1021/acs.chemrev.3c00705.
30. Dutta K, Das R, Ling J, Monibas RM, Carballo-Jane E, Kekec A, Feng DD, Lin S, Mu J, Saklatvala R, Thayumanavan S, Liang Y. In Situ Forming Injectable Thermoresponsive Hydrogels for Controlled Delivery of Biomacromolecules. *ACS Omega*, 2020 Jul 9; 5(28): 17531-17542. doi: 10.1021/acsomega.0c02009.
31. Park SH, Ji YB, Park JY, Ju HJ, Lee M, Lee S, Kim JH, Min BH, Kim MS. Injectable In Situ-Forming Hydrogels for Protein and Peptide Delivery. *Adv Exp Med Biol*, 2020; 1250: 35-48. doi: 10.1007/978-981-15-3262-7_3.
32. Coulter SM, Pentlavalli S, An Y, Vora LK, Cross ER, Moore JV, Sun H, Schweins R, McCarthy HO, Laverty G. *In Situ* Forming, Enzyme-Responsive Peptoid-Peptide Hydrogels: An Advanced Long-Acting Injectable Drug Delivery System. *J Am Chem Soc*, 2024 Aug 7; 146(31): 21401-21416. doi: 10.1021/jacs.4c03751.
33. Yen JH, Chang CC, Wu TY, Yang CH, Hsu HJ, Liou JW. Therapeutic peptides and their delivery using lipid-based nanoparticles. *Tzu Chi Med J.*, 2025 May 2; 37(3): 223-234. doi: 10.4103/tcmj.tcmj_321_24.
34. Mehrdadi S. Lipid-Based Nanoparticles as Oral Drug Delivery Systems: Overcoming Poor Gastrointestinal Absorption and Enhancing Bioavailability of Peptide and Protein Therapeutics. *Adv Pharm Bull*, 2024 Mar; 14(1): 48-66. doi: 10.34172/apb.2024.016.
35. Dhiman N, Awasthi R, Sharma B, Kharkwal H, Kulkarni GT. Lipid Nanoparticles as Carriers for Bioactive Delivery. *Front Chem*, 2021 Apr 23; 9: 580118. doi: 10.3389/fchem.2021.580118.
36. Ghasemiyeh, Parisa¹; Mohammadi-Samani, Soliman^{2, *}. Solid lipid nanoparticles and nanostructured lipid carriers as novel drug delivery systems: applications, advantages and disadvantages. *Research in Pharmaceutical Sciences*, August 2018; 13(4): 288-303. | DOI: 10.4103/1735-5362.235156
37. Niu Z, Conejos-Sánchez I, Griffin BT, O'Driscoll CM, Alonso MJ. Lipid-based nanocarriers for oral peptide delivery. *Adv Drug Deliv Rev*, 2016 Nov 15; 106(Pt B): 337-354. doi: 10.1016/j.addr.2016.04.001.
38. Hassan AAA, Ramadan E, Kristó K, Regdon G Jr, Sovány T. Lipid-Polymer Hybrid Nanoparticles as a Smart Drug Delivery System for Peptide/Protein Delivery. *Pharmaceutics*, 2025 Jun 19; 17(6): 797. doi: 10.3390/pharmaceutics17060797.

39. Schwendeman SP, Shah RB, Bailey BA, Schwendeman AS. Injectable controlled release depots for large molecules. *J Control Release*, 2014 Sep 28; 190: 240-53. doi: 10.1016/j.jconrel.2014.05.057.
40. Zhang Y, Zhang H, Ghosh D, Williams RO 3rd. Just how prevalent are peptide therapeutic products? A critical review. *Int J Pharm*, 2020 Sep 25; 587: 119491. doi: 10.1016/j.ijpharm.2020.119491.
41. Agarwal P, Rupenthal ID. Injectable implants for the sustained release of protein and peptide drugs. *Drug Discov Today*, 2013 Apr; 18(7-8): 337-49. doi: 10.1016/j.drudis.2013.01.013.
42. Wang W. Instability, stabilization, and formulation of protein pharmaceuticals. *Int J Pharm*, 2019; 568: 118503.
43. Jiskoot W, et al. Protein instability and immunogenicity: roadblocks to clinical application. *J Pharm Sci.*, 2019; 108(1): 21–30.
44. Di L, Kerns EH. Drug-like properties: concepts, structure design and methods. 2nd ed. Academic Press; 2020.
45. Makadia HK, Siegel SJ. Poly lactic-co-glycolic acid (PLGA) as biodegradable controlled drug delivery carrier. *Polymers*, 2021; 13(4): 699.
46. 6. Siepmann J, Siepmann F. Modeling of diffusion-controlled drug delivery. *J Control Release*, 2020; 314: 44–55.
47. Dash TK, Konkimalla VB. Polymeric modification and controlled drug delivery. *Drug Discov Today*, 2021; 26(1): 193–206.
48. 8. Danhier F, et al. PLGA-based nanoparticles: an overview of biomedical applications. *J Control Release*, 2021; 329: 314–339.
49. Rizzo LY, et al. Nanoparticle toxicity: focus on biocompatibility and biodegradability. *Chem Rev*, 2020; 120(6): 2705–2741.
50. 10. Rosenberg AS, et al. Immunogenicity of protein therapeutics. *Clin Pharmacol Ther*, 2019; 105(2): 269–277.
51. Baker MP, et al. Immunogenicity of therapeutic proteins: causes and mitigation strategies. *Trends Biotechnol*, 2020; 38(5): 421–434.
52. Liu M, Svirskis D, Proft T, Loh J, Yin N, Li H, Li D, Zhou Y, Chen S, Song L, Chen G, Lu WY, Zhang Z, Zhou Z, Li L, Huang Y, Bunt C, Sun G, Harris PWR, Brimble MA, Wen J. Progress in peptide and protein therapeutics: Challenges and strategies. *Acta Pharm Sin B.*, 2025 Dec; 15(12): 6342-6381. doi: 10.1016/j.apsb.2025.10.026.
53. Mehrotra S, Kalyan Bg P, Nayak PG, Joseph A, Manikkath J. Recent Progress in the Oral Delivery of Therapeutic Peptides and Proteins: Overview of Pharmaceutical Strategies to Overcome Absorption Hurdles. *Adv Pharm Bull*, 2024 Mar; 14(1): 11-33. doi: 10.34172/apb.2024.009.
54. Ebrahimi, S.B., Samanta, D. Engineering protein-based therapeutics through structural and chemical design. *Nat Commun*, 2023; 14: 2411 (). <https://doi.org/10.1038/s41467-023-38039-x>
55. Kowalczyk R, Harris PWR, Williams GM, Yang SH, Brimble MA. Peptide Lipidation - A Synthetic Strategy to Afford Peptide Based Therapeutics. *Adv Exp Med Biol*, 2017; 1030: 185-227. doi: 10.1007/978-3-319-66095-0_9. PMID: 29081055.
56. Baral KC, Choi KY. Barriers and Strategies for Oral Peptide and Protein Therapeutics Delivery: Update on Clinical Advances. *Pharmaceutics*, 2025 Mar 21; 17(4): 397. doi: 10.3390/pharmaceutics17040397.
57. Wang, Y.; Zhang, L.; Liu, C.; Luo, Y.; Chen, D. Peptide-Mediated Nanocarriers for Targeted Drug Delivery: Developments and Strategies. *Pharmaceutics*, 2025; 16: 240. <https://doi.org/10.3390/pharmaceutics16020240>
58. Liu Y, Zhao Z, Li M. Overcoming the cellular barriers and beyond: Recent progress on cell penetrating peptide modified nanomedicine in combating physiological and pathological barriers. *Asian J Pharm Sci.*, 2022 Jul; 17(4): 523-543. doi: 10.1016/j.ajps.2022.05.002.

59. Stimuli-responsive systems enable controlled release in response to specific biological or external triggers.
60. Bose D, Roy L, Chatterjee S. Peptide therapeutics in the management of metastatic cancers. *RSC Adv*, 2022 Aug 2; 12(33): 21353-21373. doi: 10.1039/d2ra02062a.
61. L. Wu, in *Peptide Therapeutics: Strategy and Tactics for Chemistry, Manufacturing and Controls*, ed. V. Srivastava, The Royal Society of Chemistry, 2019, ch. 1, pp. 1-30.
62. Vergote V, Burvenich C, Van de Wiele C, De Spiegeleer B. Quality specifications for peptide drugs: a regulatory-pharmaceutical approach. *J Pept Sci*, 2009 Nov; 15(11): 697-710. doi: 10.1002/psc.1167.
63. Patel M, Parikh D, Parihar A, Prajapati B, Patel MB, Salave S, Patel R, Malviya R, Maheshwari R, Khunt D. Protein and Peptide Therapeutics: Stability Challenges, Regulatory Demands, and Innovative Formulation Solutions for Enhanced Clinical Effectiveness. *Protein Pept Lett*, 2025; 32(7): 490-507. doi: 10.2174/0109298665375151250626124048.
64. Achilleos K, Petrou C, Nicolaidou V, Sarigiannis Y. Beyond Efficacy: Ensuring Safety in Peptide Therapeutics through Immunogenicity Assessment. *J Pept Sci*, 2025 Jun; 31(6): e70016. doi: 10.1002/psc.70016.
65. Gouveia, M.J.; Campanhã, J.; Barbosa, F.; Vale, N. From Mechanism to Medicine: Peptide-Based Approaches for Cancer Diagnosis and Therapy. *Biomolecules*, 2026; 16: 27. <https://doi.org/10.3390/biom16010027>.
66. Sahandi Zangabad P, Abousalman Rezvani Z, Tong Z, Esser L, Vasani RB, Voelcker NH. Recent Advances in Formulations for Long-Acting Delivery of Therapeutic Peptides. *ACS Appl Bio Mater*, 2023 Sep 18; 6(9): 3532-3554. doi: 10.1021/acsabm.3c00193.
67. Nakmode, D.D., Singh, B., Abdella, S. *et al.* Long-acting parenteral formulations of hydrophilic drugs, proteins, and peptide therapeutics: mechanisms, challenges, and therapeutic benefits with a focus on technologies. *Drug Deliv. and Transl. Res.*, 2025; 15: 1156–1180 (). <https://doi.org/10.1007/s13346-024-01747-y>.
68. Lei Zhou, Ting-Jie Zhang, Lu Zhang, Qiu-Ying Deng, Zhi-Yu Xia, Si-Lin Chen, Dong-Bing Cheng, Zeng-Ying Qiao, Hao Wang, Stimuli-responsive peptide-based nanodrug delivery systems for tumor therapy, *Chemical Communications*, 2025; 61(41): 7384-7407, ISSN 1359-7345, <https://doi.org/10.1039/d5cc00950b>.
69. Zhou L, Zhang TJ, Zhang L, Deng QY, Xia ZY, Chen SL, Cheng DB, Qiao ZY, Wang H. Stimuli-responsive peptide-based nanodrug delivery systems for tumor therapy. *Chem Commun (Camb)*, 2025 May 15; 61(41): 7384-7407. doi: 10.1039/d5cc00950b.
70. Omidian, H.; Wilson, R.L.; Castejon, A.M. Recent Advances in Peptide-Loaded PLGA Nanocarriers for Drug Delivery and Regenerative Medicine. *Pharmaceuticals*, 2025; 18: 127. <https://doi.org/10.3390/ph18010127>.
71. Xiao, W., Jiang, W., Chen, Z. *et al.* Advance in peptide-based drug development: delivery platforms, therapeutics and vaccines. *Sig Transduct Target Ther*, 2025; 10: 74. <https://doi.org/10.1038/s41392-024-02107-5>.
72. Ekambaram S, Dokholyan NV. Peptide-based drug design using generative AI. *Chem Commun (Camb)*, 2026 Jan 13; 62(3): 672-691. doi: 10.1039/d5cc04998a.
73. Tang S, Zhang Y, Chatterjee P. PepTune: *De Novo* Generation of Therapeutic Peptides with Multi-Objective-Guided Discrete Diffusion. *ArXiv [Preprint]*. 2025 Jun 2:arXiv:2412.17780v4.
74. Nissan, N.; Allen, M.C.; Sabatino, D.; Biggar, K.K. Future Perspective: Harnessing the Power of Artificial Intelligence in the Generation of New Peptide Drugs. *Biomolecules*, 2024; 14: 1303. <https://doi.org/10.3390/biom14101303>.

75. Yu, D.; Han, N.; Son, H.; Kim, S.J.; Kweon, S. Functional Peptide-Based Biomaterials for Pharmaceutical Application: Sequences, Mechanisms, and Optimization Strategies. *J. Funct. Biomater*, 2026; 17: 37. <https://doi.org/10.3390/jfb17010037>.
76. Al Musaimi, O. Peptide Therapeutics: Unveiling the Potential against Cancer—A Journey through 1989. *Cancers* 2024, 16, 1032. <https://doi.org/10.3390/cancers16051032>,
77. Mashhadi Abolghasem Shirazi M, Haghighat S, Nikbakht Z, Salimkia E, Kiumarsy A. Next-generation antiviral peptides: AI-driven design, translational delivery platforms, and future therapeutic directions. *Virus Res*, 2025 Nov; 361: 199642. doi: 10.1016/j.virusres.2025.199642. Epub 2025 Oct 15.

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